

This Page Is Inserted by IFW Operations
and is not a part of the Official Record

BEST AVAILABLE IMAGES

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images may include (but are not limited to):

BLACK BORDERS

- TEXT CUT OFF AT TOP, BOTTOM OR SIDES
- FADED TEXT
- ILLEGIBLE TEXT
- SKEWED/SLANTED IMAGES
- COLORED PHOTOS

BLACK OR VERY BLACK AND WHITE DARK PHOTOS

- GRAY SCALE DOCUMENTS

IMAGES ARE BEST AVAILABLE COPY.

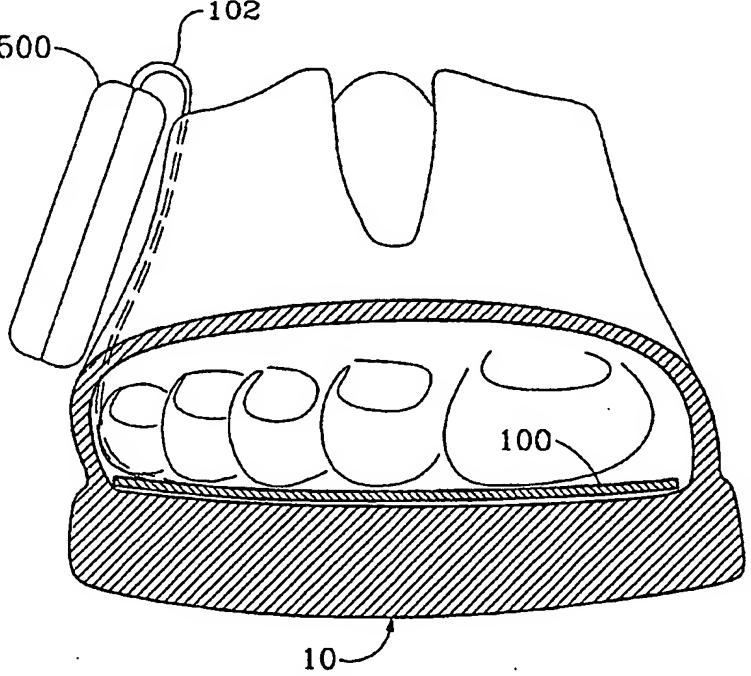
**As rescanning documents *will not* correct images,
please do not report the images to the
Image Problem Mailbox.**

PCT

WORLD INTELLECTUAL PROPERTY ORGANIZATION
International Bureau



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 5 : A61B 5/103		A1	(11) International Publication Number: WO 94/15530
			(43) International Publication Date: 21 July 1994 (21.07.94)
(21) International Application Number: PCT/US94/00536		(81) Designated States: AU, JP, US, European patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).	
(22) International Filing Date: 14 January 1994 (14.01.94)		Published <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>	
(30) Priority Data: 004,732 14 January 1993 (14.01.93) US			
(60) Parent Application or Grant (63) Related by Continuation US 004,732 (CIP) Filed on 14 January 1993 (14.01.93)			
(71) Applicant (<i>for all designated States except US</i>): FULLEN SYSTEMS, INC. [US/US]; 6302 West Alder Avenue, Littleton, CO 80123 (US).			
(72) Inventors; and (75) Inventors/Applicants (<i>for US only</i>): FULLEN, George [US/US]; 6302 West Alder Avenue, Littleton, CO 80123 (US). FULLEN, Jeryl, G. [US/US]; 1408 Terrace Drive, Newton, KS 67114 (US).			
(74) Agents: DOCKERY, David, F. et al.; Sheridan Ross & McIntosh, 1700 Lincoln Street, 35th floor, Denver, CO 80203 (US).			
(54) Title: SYSTEM FOR CONTINUOUSLY MEASURING FORCES APPLIED BY THE FOOT			
(57) Abstract			
<p>A self-contained system for measuring forces applied by the foot of a user includes a force sensor array (100) positioned within the user's shoe (10) between the foot and the inner sole of the shoe, the force sensor array including a multiplicity of individual force sensors (123) arranged in a pattern that covers the area of contact between the sole of the user's foot and the inner sole of the shoe, an electronic circuit module (500) removably attached to the side of the shoe, and a flat interconnecting cable (102) for electrically coupling the force sensor array to the electronic circuit module. An annunciator (270) audibly signals the user when a force on the foot greater than a predetermined threshold force is sensed.</p>			
 <p>The diagram illustrates a cross-section of a shoe (10) with its sole removed to reveal the internal components. A force sensor array (100) is shown as a series of interconnected circular elements embedded in the inner sole. A flat interconnecting cable (102) runs from the array to an electronic circuit module (500), which is attached to the side of the shoe. An annunciator (270) is also depicted, likely as a small speaker or microphone element.</p>			

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	GB	United Kingdom	MR	Mauritania
AU	Australia	GE	Georgia	MW	Malawi
BB	Barbados	GN	Guinea	NE	Niger
BE	Belgium	GR	Greece	NL	Netherlands
BF	Burkina Faso	HU	Hungary	NO	Norway
BG	Bulgaria	IE	Ireland	NZ	New Zealand
BJ	Benin	IT	Italy	PL	Poland
BR	Brazil	JP	Japan	PT	Portugal
BY	Belarus	KE	Kenya	RO	Romania
CA	Canada	KG	Kyrgyzstan	RU	Russian Federation
CF	Central African Republic	KP	Democratic People's Republic of Korea	SD	Sudan
CG	Congo	KR	Republic of Korea	SE	Sweden
CH	Switzerland	KZ	Kazakhstan	SI	Slovenia
CI	Côte d'Ivoire	LJ	Liechtenstein	SK	Slovakia
CM	Cameroun	LK	Sri Lanka	SN	Senegal
CN	China	LU	Luxembourg	TD	Chad
CS	Czechoslovakia	LV	Latvia	TG	Togo
CZ	Czech Republic	MC	Monaco	TJ	Tajikistan
DE	Germany	MD	Republic of Moldova	TT	Trinidad and Tobago
DK	Denmark	MG	Madagascar	UA	Ukraine
ES	Spain	ML	Mali	US	United States of America
FI	Finland	MN	Mongolia	UZ	Uzbekistan
FR	France			VN	Viet Nam
GA	Gabon				

-1-

SYSTEM FOR CONTINUOUSLY MEASURING FORCES
APPLIED BY THE FOOT

Field of the Invention

5 This invention relates generally to foot pressure sensors and more particularly to a system that may be employed by orthopedic surgeons, their patients, physical therapists, athletes, coaches, trainers, and others to measure forces applied by the foot.

10

Background of the Invention

Controlling the weight placed on an affected leg while moving about can prevent injury and speed recovery of patients recovering from certain trauma or orthopedic procedures. A person is able to perceive a changing relative weight on a foot, but cannot reliably sense how much constant weight is actually being loaded. That is, an individual's own senses cannot reliably detect how much actual constant weight he or she is placing on a foot.

15 This essential weight information must therefore be provided by some type of external or artificial device.

Forces applied by the foot are not always evenly distributed over the entire surface or sole of the foot. They are usually, but not always, concentrated at the heel or ball of the foot, and they are also usually not applied to these two areas at the same time. A typical walking or running foot strike first loads the heel and then the ball of the foot. In other situations, such as when performing an athletic maneuver, the weight placed on the foot will 25 shift in different patterns. The specific location on the

30

-2-

sole of the foot where forces are present, the times at which those forces occur, and the magnitude of those forces are of interest in a number of situations.

Many devices have been designed to measure forces applied by the foot. These include devices for measuring applied forces that are coincident with the position of the leg and body during walking or running, for measuring peak pressure to alert sensory impaired individuals such as diabetics, for measuring the total force applied by the foot, and for measuring forces applied by certain areas of the foot for various purposes.

Such foot force measurement devices are typically heavy and cumbersome and, thus, act to restrict the wearer's movements. Devices which employ an electronic package strapped to the wearer's leg above the ankle and electrically connected to a foot sensor require extra effort when attaching or removing the device. Although this extra effort may seem insignificant, it is nevertheless an inconvenience that may prompt wearer's of such devices to neglect their use. Further, these bulky devices chafe the wearer's skin, are prone to snagging, and are subject to failure resulting from stress on the electrical cable that connects the electronic package to the foot sensor. Other devices employ a stationary foot sensor pad and are therefore only suited for use in a laboratory.

All of the known foot force measurement devices function to convert mechanical force into a suitable signal medium, usually electrical signals. Consequently, the

-3-

devices can be conveniently categorized according to the type of sensor used to convert changes in mechanical force to changes in electrical signals. Accordingly, these types of sensors include pneumatic or hydraulic fluid activated switches, strain gauge sensors that respond to mechanical deformation, single direct electronic force sensors, multiple direct electronic force sensors with random spacing, and multiple direct electronic force sensors with regular spacing.

10 Pneumatic and hydraulic sensors are prone to produce inaccurate readings because changes in internal pressure are not necessarily proportional to changes in force. An accurate hydraulic sensor can be constructed if the fluid is displaced from a containing structure which itself, not
15 the fluid, supports the applied forces, and the force required to activate a switch or sensor is very small compared to the force being measured. Exemplary of such sensors are those taught in German patent 3631-923-A to Ernst and in U.S. Patent No. 3,974,491 to Sipe. Another
20 way to construct an accurate fluid sensor is to use rigid plates which limit the applied force to a constant area of fluid contact, as taught in U.S. Patent No. 3,791,375 to Pfeiffer. In such sensors, the fluid pressure is proportional to the applied force. However, these sensors
25 are disadvantageous due their bulkiness and weight.

The sensors which measure mechanical deformation of structural elements supporting the wearer's foot by use of electrical wire or ribbon type strain gauges accurately

-4-

measure weight, but they are also disadvantageous because of their bulk and weight. Exemplary of these sensors are those taught by Donald Endicott et al., "Leg Load Warning System for the Orthopedically Handicapped," Medical and 5 Biological Engineering (May, 1974), S. Miyazaki and H. Iwakura, "Foot-Force Measuring Device for Clinical Assessment of Pathological Gait," Medical and Biological Engineering and Computing (July, 1978), and G.A. Spolek and F.G. Lippert, "An Instrumented Shoe-A Portable Force 10 Measuring Device," J. Biomechanics (Great Britain, June, 1976).

All of the above-mentioned direct electronic force sensor devices are essentially identical to a type of microphone used in telephones. In this device, the acoustic 15 force compresses a partially conductive material (carbon granules) and thereby reduces its electrical resistance. A force sensor based on this concept can be constructed by forming thin electrodes on two plastic films and then covering the electrodes with a thin layer of suitable 20 partially conductive material. When the two coated films are positioned so that the two layers of partially conductive material are in contact, the electrical resistance through the sensor from electrode to electrode varies inversely with a compressing force on the sensor. 25 This is because as the coating is pressed with greater force, the electrical current path becomes broader due to increased area of contact. This effect occurs with any conductive material, but materials useful as active

-5-

elements in practical force sensors must have a relatively high electrical resistance. Such thin film electronic force sensors have the advantages of simplicity, compactness, and light weight.

- 5 Single direct electronic force sensors, such as that taught in German patent 2656-864, cannot be corrected for variations in response from one part of the sensor to another. They cannot separately measure forces on different parts of the foot. It is also possible that
10 simple bending of this type of sensor will produce a signal inappropriately indicating an applied force.

- The multiple direct electronic force sensor system taught in U.S. Patent No. 4,813,436 to Au measure forces only where the individual sensors are attached to the foot.
15 If the measurements are used to compute total force applied to the foot and are variously spaced, the contributory area of each sensor must be used in the necessary computation of the total force applied. This system is disadvantageous in that the relative position of each sensor must be
20 separately determined for each person on which the sensor is used.

- This problem is solved by the multiple direct electronic force sensors taught in U.S. Patent Nos. 4,734,034, 4,856,993, and 5,033,291 to Maness et al. in
25 which the sensors are regularly spaced. Since the relative position of each sensor is fixed, a mathematical description of the location of each sensor can easily be made part of a permanent computer database. These sensor

-6-

arrays are very thin and very light weight, but they cannot conform to a compound curved surface without wrinkling. Such wrinkled or folded thin film sensor arrays will produce erroneous results. For example, if the sensor array 5 is folded so that two separate sensors are positioned one above the other, they both measure the same force. This is an obvious error. A folded sensor array may produce an electrical signal from the folding alone, another obvious error. Folding or wrinkling also subjects the sensor array 10 to severe fatigue stress, which can lead to early and sudden failure.

A practical sensor array preferably includes several hundred individual force sensors. The problem of electrically connecting this number of individual sensors 15 to data acquisition circuitry is a significant one. A simple connection scheme would require as many electrical connections to the circuitry sensors, plus one common connection. However, the circuitry described by John A. Purbrick, "A Force Transducer Employing Conductive Silicon 20 Rubber," First Robot Vision and Sensors Conferences, Stratford-on-Avon, England (April, 1981), makes a more efficient connection method possible. This prior art circuit can measure current through individual force sensors in a two-vector array of rows and columns with a 25 top electrode of all sensors in each column commonly connected and a bottom electrode of all the sensors in each row likewise commonly connected. If such an array has equal numbers of columns and rows, the number of connections to

-7-

circuitry is reduced to twice the square root of the number of sensors. The Purbrick method is not as efficient when employing other ratios of columns to rows of sensors, but it nevertheless represents an efficient method for 5 interconnecting the sensor array of the present invention. A similar method is taught by W.D. Hillis, "Active Touch Sensing," Artificial Intelligence Laboratory Memo 629, M.I.T. (April, 1981).

10

Summary of the Invention

It would therefore be advantageous to provide a self-contained force measurement system for continuously sampling the magnitude and distribution of forces that are present on the bottom of one or both feet of the user when 15 engaged in various activities.

It would further be advantageous to provide such a force measurement system that does not unduly impede walking, running or other ordinary movements of the user.

It would further be advantageous to provide such a 20 force measurement system that is self-contained for use away from a laboratory or clinic and that is capable of annunciating appropriate weight bearing conditions, of generating computer data for future reference and analysis, and be capable of transmitting this computer data by 25 wireless means to remotely located equipment.

Devices in accordance with the present invention provide a force measurement system useful to the medical patient, attendant physician, physical therapist,

-8-

prosthetist, orthotist, podiatrist, athlete, sports trainer, coach or research professional interested in carefully studying or managing a wide range of problems of the human lower extremity.

- 5 In accordance with an embodiment of the present invention, a self-contained system is provided for measuring forces applied by the foot of a user, whereby a force sensor array is positioned relative to a user's foot, thus allowing the measurement of the forces applied by the
- 10 foot as weight is applied while the user is standing, walking or running. The force sensor array is comprised of a multiplicity of individual force sensors arranged so the force sensor array will operatively conform to the user's foot where the force is applied. Furthermore, a force
- 15 analysis unit is provided for measuring the force applied to the force sensor array by the user as well as an interconnection device for transferring one or more signals related to the force from the sensor array to the force analysis unit or electronic circuit module. The force
- 20 analysis unit primarily serves the purpose of substantially continuously monitoring signals from the force sensor array to obtain information which is indicative of the force sensed by each individual force sensor on a multiplicity of force sensors which make up the force sensor array.
- 25 In accordance with an additional embodiment of the present invention, the individual force sensors are arranged in a wrinkle resistant pattern that covers a substantial area of contact of the user's foot. This

-9-

prevents inadvertent force readings as a result of wrinkling under the foot.

In accordance with an additional embodiment of the present invention, the force sensor array is comprised of 5 a substrate material so rigid as to not operatively conform to the foot in the absence of a removed cutout portion. This cutout portion of the substrate material allows the force sensor array to operatively conform to the user's foot when force is applied, thus providing additional 10 comfort to the user. Furthermore, these cutouts provide flexibility to the force sensor array, thus preventing wrinkling and subsequent damage to the force sensor array or erroneous force readings.

In accordance with a more preferred embodiment of the 15 present invention, an electronic circuit module, or force analysis means, is adapted for removable attachment to foot related apparel, such as a shoe, bootie, slipper or prosthetic device.

In accordance with a more preferred embodiment of the 20 present invention, the force analysis unit is comprised of scanning circuitry for scanning the force sensor array and a central processing unit for executing instructions and controlling the scanning circuitry and for processing force and pressure information provided by either one or a 25 multiplicity of force sensors in the force sensor array. Furthermore, a read-only memory device is coupled to the central processing unit for storing programs and subroutines of instructions to be executed by the central

-10-

processing unit during a system boot period of operation. Additionally, a random access memory unit is provided for storing additional routines and subroutines of instructions to be executed by the central processing unit subsequent to 5 the system boot period of operation and for storing the usage data.

In accordance with a preferred embodiment of the present invention, a clock or time measuring device is attached to the central processing unit for providing date 10 and time of day information thereto. This allows therapists or doctors to evaluate when the force sensing unit was used and for what duration and when forces were applied.

In accordance with an improved embodiment of the present invention, an annunciator device such as a beeper 15 or horn is used which provides an audible signal to the user during certain preprogrammed system operating conditions. Further, the central processing unit may be programmed for accumulating the forces sensed by each one or by a multiplicity of individual force sensors in the 20 force array which can compare the accumulated force to a predetermined threshold force. If the accumulated force exceeds the predetermined threshold force, the annunciator will audibly provide a signal to the user.

In accordance with a further improved embodiment of 25 the present invention, a wireless data transmitter unit is provided for coupling the central processing unit to a remotely located computer, thus enabling the transfer of

-11-

selected information, including the force data, between the central processing unit and the external computer.

In accordance with a preferred embodiment of the present invention, a force sensor array is provided which 5 is positioned relative to a user's foot to measure the forces applied by the user. This force sensor array is comprised of both top and bottom electrode layers, the top and bottom layers including corresponding pluralities of substantially vertically coincident and individual sensor 10 electrodes. The pluralities of individual sensor electrodes of each of the top and bottom electrode layers are arranged to form lines of sensor electrodes and the individual sensor electrodes of a given line of sensor electrodes are electrically serially connected by a conductive trace that 15 follows a substantially nonlinear path. Furthermore, at least one partially conductive pressure sensitive coating is sandwiched between the top and bottom electrode layers. Accordingly, there are both top and bottom substrate layers overlying the top and bottom electrode layers, 20 respectively, each of the top and bottom substrate layers comprising a plurality of geometric cutouts in areas not directly overlying the pluralities of individual sensor electrodes. The cutouts in the substrate serve the purpose of allowing the force sensor array to stretch in multiple 25 horizontal directions simultaneously and to operatively conform to the user's foot when pressure is applied.

Furthermore, the system includes top and bottom conductive trace layers overlying the top and bottom

-12-

electrode layers, respectively, each of the top and bottom conductive trace layers including a plurality of conductive traces, and each of the conductive traces being electrically connected through a corresponding one of the 5 top and bottom substrate layers to a particular one of the lines of sensor electrodes of a corresponding one of the top and bottom electrode layers.

In accordance with a more preferred embodiment of the present invention, the individual sensor electrodes are 10 spaced horizontally equidistant apart.

In accordance with yet a more preferred embodiment of the present invention, the pluralities of the individual sensor electrodes of each of the top and bottom electrode layers are arranged to form substantially parallel 15 equidistant lines of sensor electrodes positioned diagonally with respect to a longitudinal axis of the shoe.

In accordance with an additional embodiment of the present invention, each of the top and bottom substrate layers comprises a dielectric film.

20 In accordance with yet another embodiment of the present invention, each of the top and bottom substrate layers comprises a partially conductive pressure sensitive coating.

25 In accordance with a preferred embodiment of the present invention, each one of the plurality of cutouts in each of the top and bottom substrate layers is hexagonal in shape.

-13-

In accordance with another preferred embodiment of the present invention, each one of the plurality of cutouts in each of the top and bottom substrate layers is shaped in a modified hourglass configuration.

5 In accordance with a preferred embodiment of the present invention, a self-contained system for measuring forces applied by the foot of a user comprises a force sensor array positioned relative to a user's foot, the force sensor array comprising a multiplicity of individual
10 force sensors arranged in a predetermined wrinkle resistant pattern that covers a substantial area of contact of the user's foot such that the force sensor array operatively conforms to the user's foot where force is applied.

Furthermore, the force sensors comprise a top and
15 bottom electrode layer with the top and bottom electrode layers including corresponding pluralities of substantially vertically coincident spaced individual sensor electrodes. These pluralities of individual sensor electrodes of each of the top and bottom electrode layers are arranged to form
20 substantially parallel equidistant lines of sensor electrodes positioned diagonally with respect to a longitudinal axis of the shoe. Further, the individual sensor electrodes of a given diagonal line of sensor electrodes are electrically serially connected by a
25 conductive trace that follows a substantially nonlinear path.

-14-

Additionally, at least one partially conductive pressure sensitive coating is sandwiched between the top and bottom electrode layers.

Furthermore, top and bottom substrate layers overlay 5 the top and bottom electrode layers, respectively, each of the top and bottom substrate layers comprising a lattice structure having a plurality of cutouts in areas not directly overlying the pluralities of individual sensor electrodes. These cutouts are provided to allow the force 10 sensor array to stretch in multiple horizontal directions simultaneously and to conform to the user's foot when pressure is applied.

Additionally, top and bottom conductive trace layers are provided which overlay the top and bottom electrode 15 layers, respectively. Each of the top and bottom conductive trace layers include a plurality of conductive traces and each of the conductive traces are electrically connected through a corresponding one of the top and bottom substrate layers to a particular one of the diagonal lines of sensor 20 electrodes of a corresponding one of the top and bottom electrode layers.

Furthermore, the force analysis unit for measuring a force applied to the force sensor array is adapted for attachment to foot related apparel and a method of 25 interconnecting is provided for transferring one or more signals related to the force from the sensor array to the force analysis unit. The force analysis unit is operative for substantially continuously monitoring signals from the

-15-

force sensor array to obtain information indicative of force sensed by the multiplicity of individual force sensors comprising the force sensor array.

In accordance with an additional embodiment of the
5 present invention, a force sensor array is provided which comprises a first signal conducting plurality of spaced apart pressure sensing signaling devices so that a signal from each device relates to a force applied thereto. Furthermore, a second signal conducting plurality of spaced
10 apart pressure sensing signaling devices are provided so that a first signal between a first device from the first plurality and a second device from the second plurality uniquely determines a force applied to the first and second devices. Thus, the first and second signal conducting
15 pluralities are each arranged in diagonal rows in relation to a longitudinal axis of the array so that the devices in each row are electrically serially connected by a different conductive trace for transmission of a signal related to a force applied thereto. Furthermore, the system includes a
20 partially conductive pressure sensitive device conducting the first signal between the first and second devices, and additionally including a substrate material attached to the first and second signal conducting pluralities, the substrate having a plurality of shaped cutouts allowing the
25 force sensor array to smoothly conform to a pressure-applying object when pressure is applied. Additionally, the substrate contacts the first and second signal conducting pluralities in a manner capable of conducting a

-16-

force to the first and second devices, wherein the conductive traces traverse a thickness of the substrate. Additionally, each first conductive trace connected to a first row of the first signal conducting plurality is capable of transmitting an electrical signal to a second conductive trace connected to a second row of the second signal conducting plurality through a unique pair of pressure sensing devices, one pressure sensing device of the pair from the first row and one pressure sensing device of the pair from the second row.

In accordance with a preferred embodiment of the present invention, the force sensor array includes diagonal rows for the first signal conducting plurality directed in a first direction while the diagonal rows for the second signal conducting plurality are directed in a second direction with the first and second directions substantially different.

Brief Description of the Drawings

Figure 1 is a pictorial diagram of a shoe fitted with a force sensor array and an interconnected electronic circuit module in accordance with the present invention.

Figure 2 is a partial sectional pictorial diagram of the shoe of Figure 1 illustrating the position of the force sensor array within the shoe.

Figure 3 is an exploded sectional diagram of the force sensor array employed within the shoe of Figures 1 and 2.

-17-

Figure 4 is a detailed diagram of a portion of the force sensor array of Figure 3 illustrating the planar arrangement of the conductive traces forming the top and bottom sensor electrodes and their relationship to pressure sensitive conductive coatings and removed areas of the substrates.

Figure 5 is a detailed diagram illustrating conductive traces on a top surface of a top substrate of the force sensor array of Figure 3.

Figure 6 is a detailed diagram illustrating conductive traces on a bottom surface of the top substrate of the force sensor array of Figure 3.

Figure 7 is a detailed diagram illustrating conductive traces on a top surface of a bottom substrate of the force sensor array of Figure 3.

Figure 8 is a detailed diagram illustrating conductive traces on a bottom surface of the bottom substrate of the force sensor array of Figure 3.

Figure 9 is a sectional diagram illustrating the details of the interconnection between the force sensor array and electronic circuit module of Figures 1 and 2.

Figure 10 is an exploded pictorial diagram of the interconnection of Figure 9.

Figure 11 is a block diagram of circuitry employed in the electronic circuit module of Figures 1 and 2.

Figure 12 is a flow chart of a software routine performed by the circuitry of Figure 11 within the electronic circuit module of Figures 1 and 2 to enable the

-18-

foot force measurement system of the present invention to function as a weight monitor.

Figure 13 is a detailed diagram illustrating the substrate material, force sensors, and a modified hourglass 5 cutout configuration in the force sensor array.

Detailed Description of the Preferred Embodiment

Referring now to Figures 1 and 2, there is shown a shoe 10 containing a force sensor array 100 and an 10 electronic circuit module 500 connected thereto by means of a flat ribbon cable 102. Force sensor array 100 is arranged to cover a substantial area of contact between the bottom of the wearer's foot and foot apparel (e.g., shoe) 10. Although the use of a force sensor array in a shoe 15 represents a preferred embodiment of the present invention, many similar types of foot apparel may utilize the same type of system. For example, the force sensor array may be used inside a sock, bootie, or attached to a prosthetic device to accomplish the same result of measuring and 20 monitoring forces applied by the user's foot.

Additionally, although the preferred embodiment involves the measurement of forces between a foot and shoe, it should be appreciated that this device could be used to measure other forces, such as between the end of an 25 amputated limb and a prosthetic device.

Electronic circuit module 500 is preferably clipped or otherwise attached to the side of shoe 10 that is opposite the other foot and slightly forward of the center thereof,

-19-

where it is least likely to be damaged or to interfere with the normal physical activities of the wearer.

Referring now to Figure 3, covering layers 112 and 142 are used to hold the remaining parts of the force sensor array 100 together and to isolate them from contamination. Covering layers 112 and 142 can include, for example, a 1/16-inch thick, adhesive coated, closed cell vinyl foam tape such as 3M Scotchfoam 4726™. A conductive trace layer 122 includes a multiplicity of conductive traces, each of which is electrically connected through a substrate 124 to each line of a multiplicity of lines of sensor electrodes (123 in Figure 4) that are formed by a conductive trace layer 126 and a like number of contact points that are also formed by conductive trace layer 126. Similarly, a conductive trace layer 132 includes a multiplicity of conductive traces, each of which is electrically connected through a substrate 134 to each line of a multiplicity of lines of sensor electrodes (123 in Figure 4) formed by another conductive trace layer 136. Conductive trace layers 122, 126, 132, and 136 can be fabricated from any suitable electrically conductive material capable of being printed or otherwise deposited on substrates 124, 134. Substrates 124, 134 are dielectric films and can be fabricated from, for example, du Pont Kapton™ polyimide film material. Other films can also be used. Preferably, substrates 124 and 134 are fabricated from materials which are too rigid to operatively conform to a user's foot when no portions have been removed therefrom. However, when

-20-

selected portions of substrates 124 and 134 are removed, as shown in Figures 5 and 13, the substrates are capable of operatively conforming to the user's foot, while simultaneously avoiding undesirable wrinkling. Pressure 5 sensitive coating layers 128, 138 can comprise a commercially available partially conductive pressure sensitive coating, such as one of those designated as numbers 4407 and 4408 produced by Chomerics, Inc. of Woburn, MA.

10 Referring now to Figure 4, hexagonal areas 130 of the substrates 124, 134 are removed to increase the flexibility of the assembled force sensor array 100, allow it to operatively conform to the user's foot, provide mechanical isolation for the individual sensors 123 comprising force 15 sensor array 100, and allow contact of the adhesive coatings 114, 144. Although hexagonal cutouts 130 are a preferred embodiment of the present invention, any suitable geometric shape of cutout can be utilized which enhances the flexibility of the force sensor array 100. The actual 20 geometric configuration is dependent on a number of variables including the substrate material, thickness of the substrate and total length and width of the material necessary for each particular application. Conductive trace layers 126, 136, which form individual force sensor 25 electrodes 123, are prevented from directly contacting each other by the position and shape of pressure sensitive coatings 128, 138. The areas of the partially conductive pressure sensitive coatings 128, 138 are slightly larger

-21-

than the sensor electrode areas, and the conductive traces connecting the individual force sensor electrodes 123 not covered by the pressure sensitive coatings 128, 138 do not come into contact because their positions are not
5 coincident. The film substrates 124, 134 between the hexagonal or other geometric removed areas are wide enough to accommodate the various conductive traces, electrodes, and sensor areas. Narrower bands of the film substrates 124, 134 between the individual force sensors 123 of force
10 sensor array 100 result in greater flexibility and provide better mechanical isolation of the individual sensors.

Referring now to Figure 5 and 6, conductive trace layer 122 on the top surface of film substrate 124 connects each line 121 of individual force sensor electrodes 123 formed by conductive trace layer 126 on the bottom surface of film substrate 124 to the electronic circuit module 500 of Figures 1 and 2. Electrical connections through the film substrate to conductive trace layer 126 on the bottom surface of film substrate 124 are represented as enlarged areas 117 at both ends of each conductive trace 101 of conductive trace layer 122.
15
20

Referring now to Figure 6, conductive trace layer 126 forms diagonal lines 121 of sensor electrodes 123 and contact areas for connection to the electronic circuit module 500. Electrical connections through the substrate 124 to conductive trace layer 122 on the top surface of film substrate 124 are represented as enlarged areas 127 located firstly between consecutive force sensor electrodes
25

-22-

123 and secondly under the contact areas 125 in connector tab 104. Thus, all of the individual force sensor electrodes 123 in a diagonal line 121 are commonly connected through a single conductive trace 101 of 5 conductive trace layer 122 to electronic circuit module 500.

Referring now to Figure 7, conductive trace layer 136 forms lines of individual force sensor electrodes and contacts for connection to the electronic circuit module 10 500. Electrical connections through the substrate 134 to conductive layer 132 are represented as enlarged areas located firstly between consecutive individual force sensor electrodes and secondly under the contact areas of conductive trace layer 136 in connector tab 104. Thus, all 15 of the individual force sensor electrodes in a line are commonly connected through a single conductive trace of conductive trace layer 132 to electronic circuit module 500.

Referring now to Figure 8, conductive traces of 20 conductive trace layer 132 connect each line of individual force sensor electrodes formed by conductive trace layer 136 to the electronic circuit module 500. Electrical connections through the substrate 134 to conductive trace layer 136 are represented as enlarged areas at both ends of 25 each trace of layer 132.

Referring now generally to Figures 5-8, the layout of the force sensors 123, lines of individual force sensor electrodes formed by conductive traces of conductive trace

-23-

layers 126, 136, and conductive traces 122, 132 permit trimming the array to fit any shape or size of a user's foot or shoe. The diagonal arrangement of force sensors 128, 138 results in a smaller number of electrical leads in 5 conductive trace layers 122, 132 than would be required if the sensors 128, 138 were perpendicularly arranged. This is because the ratio of the length to width of the human foot is about 3.5, and a similar ratio of rows to columns would result. In the diagonal sensor layout of the present 10 invention, the ratio of rows to columns can be closer to unity. The honeycomb pattern of the substrates produces meandering nonlinear courses for electrical conductive leads in conductive trace layers 122, 132. This prevents a stiff conductive material such as copper from excessively 15 restricting the flexing of the force sensor array 100 along the general direction of the leads.

Referring now to Figures 9 and 10, a portion of a standard two-sided printed circuit board 550 extends to the exterior periphery of electronic circuit module 500, 20 together with conductive leads 552 to form contacts arranged to coincide with contact areas of electrode lines formed by conductive trace layers 126, 136. The connector portion of force sensor array 100 and the printed circuit board 550 are clamped between facing halves 502 of 25 electronic circuit module 500. Any conventional mechanical fastening device may be used to hold the facing halves 502 of electronic circuit module 500 together. Elastic material 504 evenly distributes the clamping force. A thickened

-24-

center of elastic material 504 compensates for any bending that may take place in the two facing halves 502 of electronic circuit module 500. Guides 506 position the end portions of the force sensor array 100, while the two 5 facing halves 502 of electronic circuit module 500 are tightened. The clearance between the connector parts 104 of substrates 124, 134 to guides 506 is small enough to assure alignment between each of the connector contact areas of electrode lines formed by conductive trace layers 10 126, 136 and contact areas 552. The conductive traces of conductive trace layers 122, 132 are as closely spaced as practical to make the cable 102 portion of substrates 124, 134 as narrow as possible. Curving the re-entrant edges of substrates 124, 134 reduces fatigue stress.

15 Referring now to Figure 11, force sensor array 100 is connected to electronic circuit module 500, which contains scanning circuitry 210 controlled by a central processing unit (CPU) 220. CPU 220 executes software routines stored in a read-only memory (ROM) 230 during system boot and 20 thereafter executes software programs stored in a random access memory (RAM) 250. An interface 240 is used to upload data stored in RAM 250 to an external personal computer (PC) and to down-load operational data and software programs from a PC to RAM 250. A time of day and 25 calendar clock 260 provides time and date information to CPU 220. An annunciator 270 is controlled by CPU 220 for signalling, for example, the occurrence of measured forces exceeding preset thresholds, hardware fault conditions, and

-25-

operator errors. In addition, a wireless data transmitter (not shown) may be included to interface electronic circuit module 500 to external electronic equipment for the purpose of transferring data and other information between 5 electronic circuit module 500 and the external electronic equipment.

Referring now to Figure 12, there is shown a software program executed by CPU 220 contained within electronic circuit module 500 to facilitate operation of the foot force measurement system of the present invention as a weight monitor. Initialization step 302 can be a conventional software initialization step involving setting memory areas to proper values, checking hardware configurations, etc. Step 304 reads one byte of data from 10 the scanning circuitry 210. This data represents either the result of a single instantaneous reading from an individual sensor within force sensor array 100 or a special synchronizing value to mark the beginning or end of a scan of the entire force sensor array 100. Step 306 tests the 15 data byte for the special value. When this value is the special synchronizing value, the next byte of data read will be force data from a known sensor of force sensor array 100. The next byte is not read until it is time to do so, as determined by steps 307 and 308. The force sensor 20 array 100 can be scanned many times per second. The loop formed by steps 310-318 is executed as many times as there 25 are individual sensors within the force sensor array 100. The current through each of the sensors of force sensor

-26-

array 100 is measured in a predetermined order and consequently the individual force sensor being addressed can be associated to stored data representing its location within the force sensor array 100. Step 312 tests for the 5 special synchronizing byte, and if it is found at this point in the routine, it is a clear error. Step 314 makes an appropriate data record for future reference, announces the error, and resets a loop counter to point to the first sensor.

10 Step 316 extracts information stored in RAM 250 for the particular sensor of force sensor array 100 currently being evaluated. This information is used to translate the measured current through an individual sensor to a value accurately representing the force being placed on that 15 sensor. This is necessary because the output voltage of each sensor of the force sensor array 100 is inversely and logarithmically proportional to the applied force, and the response varies between individual sensors due to unavoidable manufacturing variances. More specifically, 20 within the RAM 250 is stored a two-vector data array previously loaded by use of a PC and other suitable test equipment. In this array, a first vector applies to each sensor, and a second vector applies to each possible input data value from a particular sensor. Contained in each 25 storage location within the data array is the appropriate output value. Stated in other words, a counter incremented with each iteration of the loop comprising steps 310, 312, 314, 316 and 318 is taken as a first pointer and the value

-27-

from the sensor measurement is taken as a second pointer to the proper output data stored in the two-vector data array. The value pointed to is added to the value representing the total weight measured by the force sensor array 100.

- 5 Following execution of the loop comprising steps 310, 312, 314, 316 and 318, a single scan of the force sensor array 100 has been completed, and the total force on the force sensor array 100 has been computed.

Steps 320, 322, 324, 326, 328, and 330 serve to test
10 the total instantaneous force from the scan of the force sensor array 100 against two preset values stored in RAM 250. If a "maximum allowable force" (MAF) has been exceeded, a recognizable tone is produced by the annunciator 270. If the total force is less than the MAF,
15 but greater than a predetermined proportion of the MAF, a clearly different tone is produced. If the total force is less than the predetermined proportion of the MAF, no tone is produced. Alternatively, the program can be designed to monitor forces in desired localized areas rather than over
20 the entire foot. Step 305 clears the storage location for total force. Since the next byte should be a synchronizing byte, it must be wasted. This is done by step 304 before beginning execution of the next loop comprising steps 310, 312, 314, 316 and 318.

- 25 Referring now to Figure 13, modified hourglass cutouts 199 are removed from the film substrate 124, 134 to increase the flexibility of the force sensor array and allowing it to operatively conform to the user's foot yet

-28-

provide mechanical isolation for the pressure sensitive coating layers 128, 138. The actual geometric configuration of the cutout may change depending on the substrate material used and the length, width and thickness of the
5 material.

In use, the foot force measurement system described above is capable of measuring the instantaneous force on all of the individual force sensors within force sensor array 100 during a scan that takes place at regular,
10 predetermined time intervals. The scan rate is fast enough to assure a multiplicity of scans for any foot strike and thus capture any significant instantaneous force value. Consequently, a time-based plot of force on the entire foot or any part thereof may be produced for each foot strike.
15 The force centroid or balance point of forces placed on a foot or portions of a foot may be computed for each scan of force sensor array 100 because the relative position of each of the sensors within force sensor array 100 is fixed. Therefore, a time-based two-coordinate plot of the path of
20 the centroid may be produced for each foot strike. Force placed on the foot in excess of that required to counteract the individual's weight may be assumed to be due to acceleration resulting from work done by that individual. This acceleration can be used to compute an instantaneous
25 resultant velocity from which the mechanical power produced by the individual can be computed. Using these primary measurements and computations, information can be produced

-29-

which is useful in circumstances including but not limited to those discussed below.

The foot force measurement system of the present invention may be used as a foot force monitor by persons 5 with prosthetic bone or joint implants and fractures who need to carefully control the weight placed on an affected leg during a recovery period. The individual uses crutches or a walker for physical support and, guided by audible tones from the annunciator 270, can control the amount of 10 weight placed on the affected leg. In addition to announcing individually set optimum and excessive weight thresholds, the foot force measurement system of the present invention also has the capability of generating and storing computer data records which, for example, may 15 include the date and time of system turn on and turn off, and the number of foot strikes of a minimum useful force. When the stored data is reviewed following a period of usage that may extend for several weeks, for example, clear indications are provided regarding the extent of system 20 usage and adherence by the wearer to a prescribed course of therapy.

The foot force measurement system of the present invention may also be used to alert the staff of a nursing center when patients who are prone to confusion or are 25 otherwise at risk of falling attempt to stand and walk without assistance. When the patient first places weight on either foot in an effort to stand, the force is detected by the force sensor array 100 fitted into flexible footwear

-30-

typically worn by such patients. This would trigger a suitable display and annunciator on a computer console located at the central nurses' station to provide an early warning of a patient's attempt to rise from his or her bed.

5 The foot force measurement system of the present invention may also find application as a guide to fitting and adjustment of a prosthetic leg. It may also be used in training a patient in use of a prosthesis. In this instance, the force sensor array 100 can be placed between
10 the prosthetic foot and a shoe or between the end of the limb and the prosthetic device.

The foot force measurement system of the present invention may also be used to provide runners and other athletes instantaneous and continuous measurements of their
15 power output and pace, as measured by frequency of foot strikes. These measurements can be compared to historical values for the current wearer and others so that appropriate and timely adjustments in pace or other running techniques may be made. Deviations of force centroid path
20 or force-time curve from normal values for the individual wearer can be detected. Such deviations imply impending injury, and when they occur, a warning may be sounded in time to avoid an injury.

The foot force measurement system of the present
25 invention may also find application in weight loss programs to monitor the wearer's compliance with an established exercise schedule.

-31-

The foot force measurement system of the present invention may be used to detect lower extremity abnormalities or improper footwear and to monitor the result of corrective measures. This is done by comparing a patient's force-time plot(s) and/or the force centroid path plot with normal plots of these parameters. The precise functional information provided by the system of the present invention can be used to quantify and display well-understood anatomical conditions. Use of the present invention to measure and chart a statistically significant number of subjects could produce detailed standards for subsequent comparison not otherwise available. By comparing individual plots with known standards developed through use of the foot force measurement system of the present invention, a wider range of problems could be detected earlier and more accurately than is presently possible.

While the invention has been described in combination with specific embodiments thereof, it is evident that many alternatives, modifications and variations will be apparent to those skilled in the art in light of the foregoing description. Accordingly, it is intended to embrace all such alternatives, modifications, and variations as fall within the spirit and broad scope of the claims.

-32-

What is claimed is:

1. A self-contained system for measuring forces applied by the foot of a user, the system comprising:

(a) a force sensor array positioned relative to a user's foot so as to measure the forces applied by said foot, said force sensor array comprising a multiplicity of individual force sensors arranged such that said force sensor array conforms to the user's foot where force is applied;

10 (b) force analysis means for monitoring signals from said force sensor array to obtain information indicative of force sensed by said multiplicity of individual force sensors comprising said force sensor array; and

15 (c) interconnection means for transferring one or more signals related to the force from said force sensor array to said force analysis means.

2. The system as claimed in claim 1, wherein said individual force sensors are arranged in a wrinkle resistant pattern that covers a substantial area of contact 20 of the user's foot.

3. The system as claimed in claim 1, wherein said force sensor array comprises a substrate material which is so rigid that it will not operatively conform to the user's foot unless a cutout portion of said substrate material is 25 removed in order to allow said force sensor array to operatively conform to the user's foot when force is applied.

-33-

4. The system as claimed in claim 1, wherein said force analysis means is adapted for removable attachment to foot related apparel.

5. The system as claimed in claim 1, wherein said force analysis means comprises:

(a) scanning circuitry for scanning said force sensor array;

10 (b) central processing means for executing instructions controlling said scanning circuitry and for processing said information indicative of the force sensed by said multiplicity of individual force sensors comprising said force sensor array to obtain force data;

15 (c) read-only memory means coupled to said central processing means for storing routines and subroutines of instructions to be executed by said central processing means during a system boot period of operation; and

20 (d) random access memory means for storing additional routines and subroutines of instructions to be executed by said central processing means subsequent to said system boot period of operation and for storing said force data.

6. The system as claimed in claim 5, further comprising clock means coupled to said central processing means for providing date and time of day information thereto.

25 7. The system as claimed in claim 5, further comprising:

annunciator means for providing an audible signal to the user during certain system operating conditions;

-34-

wherein said central processing means is operative for accumulating said force sensed by at least one of said multiplicity of individual force sensors and for comparing the accumulated force to a predetermined threshold force 5 and for causing said annunciator means to audibly indicate an accumulated force that exceeds said predetermined threshold force.

8. The system as claimed in claim 5, further comprising wireless data transmitter means for coupling 10 said central processing means to a remotely located computer to enable the transfer of selected information, including said force data, between said central processing means and said external computer.

-35-

9. A force sensor array comprising:

- (a) top and bottom electrode layers, said top and bottom electrode layers including corresponding pluralities of substantially vertically coincident individual sensor electrodes, the pluralities of individual sensor electrodes of each of said top and bottom electrode layers being arranged to form lines of sensor electrodes, the individual sensor electrodes of a given line of sensor electrodes being electrically serially connected by a conductive trace
5 that follows a substantially nonlinear path;
- (b) at least one partially conductive pressure sensitive coating sandwiched between said top and bottom electrode layers;
- (c) top and bottom substrate layers overlying said
15 top and bottom electrode layers, respectively, each of said top and bottom substrate layers comprising a plurality of cutouts in areas not directly overlying said pluralities of individual sensor electrodes, said cutouts allowing the
force sensor array to stretch and flex in multiple
20 horizontal directions simultaneously and to conform to the shape of the pressure-applying object when pressure is applied; and
- (d) top and bottom conductive trace layers overlying said top and bottom electrode layers, respectively, each of
25 said top and bottom conductive trace layers including a plurality of conductive traces, each of said conductive traces being electrically connected through a corresponding one of said top and bottom substrate layers to a particular

-36-

one of the said lines of sensor electrodes of a corresponding one of said top and bottom electrode layers.

10. The system as claimed in claim 9, wherein said individual sensor electrodes are spaced horizontally
5 equidistant apart.

11. The system as claimed in claim 9, wherein the pluralities of said individual sensor electrodes of each of said top and bottom electrode layers are arranged to form substantially parallel equidistant lines of sensor
10 electrodes positioned diagonally with respect to a longitudinal axis of said shoe.

12. The system as claimed in claim 9, wherein each of said top and bottom substrate layers comprises a dielectric film.

15 13. The system as claimed in claim 9, wherein each of said top and bottom substrate layers comprises a partially conductive pressure sensitive coating.

14. The system as claimed in claim 9, wherein each one of said plurality of cutouts in each of said top and
20 bottom substrate layers is hexagonal in shape.

15. The system as claimed in claim 9, wherein each one of said plurality of cutouts in each of said top and bottom substrate layers is a modified hourglass configuration.

-37-

16. A self-contained system for measuring forces applied by the foot of a user, said system comprising:

(a) a force sensor array positioned for contact with the bottom of a user's foot, said force sensor array
5 comprising a multiplicity of individual force sensors arranged in a wrinkle resistant pattern that covers a substantial area of contact of the user's foot such that said force sensor array operatively conforms to the user's foot where force is applied;

10 (b) said force sensors comprising:

(i) top and bottom electrode layers, said top and bottom electrode layers including corresponding pluralities of substantially vertically coincident spaced individual sensor electrodes, the pluralities of individual sensor
15 electrodes of each of said top and bottom electrode layers being arranged to form substantially parallel equidistant lines of sensor electrodes positioned diagonally with respect to a longitudinal axis of said shoe, the individual sensor electrodes of a given diagonal line of sensor
20 electrodes being electrically serially connected by a conductive trace that follows a nonlinear path;

(ii) at least one partially conductive pressure sensitive coating sandwiched between said top and bottom electrode layers;

25 (iii) top and bottom substrate layers overlying said top and bottom electrode layers, respectively, each of said top and bottom substrate layers comprising a lattice structure having a plurality of cutouts in areas not

-38-

directly overlying said pluralities of individual sensor electrodes, said cutouts allowing the force sensor array to stretch and flex in multiple horizontal directions simultaneously and to conform to the user's foot when
5 pressure is applied; and

(iv) top and bottom conductive trace layers overlying said top and bottom electrode layers, respectively, each of said top and bottom conductive trace layers including a plurality of conductive traces, each of
10 said conductive traces being electrically connected through a corresponding one of said top and bottom substrate layers to a particular one of the said diagonal lines of sensor electrodes of a corresponding one of said top and bottom electrode layers; and

15 (c) force analysis means for measuring a force applied to said force sensor array, adapted for attachment to foot related apparel; and

(d) interconnection means for transferring one or more signals related to the force from said sensor array to
20 said force analysis means, said force analysis means being operative for substantially continuously monitoring signals from said force sensor array to obtain information indicative of force sensed by said multiplicity of individual force sensors comprising said force sensor array.
25

-39-

17. A force sensor array, comprising:

(a) a first signal conducting plurality of spaced apart pressure sensing signaling devices so that a signal from each said devices relates to a force applied thereto;

5 (b) a second signal conducting plurality of spaced apart pressure sensing signaling devices so that a first signal between a first device from said first plurality and a second device from said second plurality uniquely determines a force applied to said first and second

10 devices;

wherein said first and second signal conducting pluralities are each arranged in diagonal rows in relation to a longitudinal axis of the array so that the devices in each row are electrically serially connected by a different

15 conductive trace for transmission of a signal related to a force applied thereto;

(c) a partially conductive pressure sensitive means conducting the first signal between said first and second devices;

20 (d) substrate means attached to said first and second signal conducting pluralities, said substrate having a plurality of shaped cutouts allowing said force sensor array to smoothly conform to a pressure-applying object when pressure is applied, said substrate contacting said

25 first and second signal conducting pluralities in a manner capable of conducting a force to said first and second devices;

-40-

wherein said conductive traces traverse a thickness of said substrate; and

wherein each first said conductive trace connected to a first row of said first signal conducting plurality is capable of transmitting an electrical signal to a second said conductive trace connected to a second row of said second signal conducting plurality through a unique pair of said pressure sensing devices, one said pressure sensing device of said pair from said first row and one said pressure sensing device of said pair from said second row.

18. A force sensor array as claimed in claim 17, wherein said diagonal rows for said first signal conducting plurality are directed in a first direction and said diagonal rows for said second signal conducting plurality are directed in a second direction, said first and second directions substantially different.

1 / 10

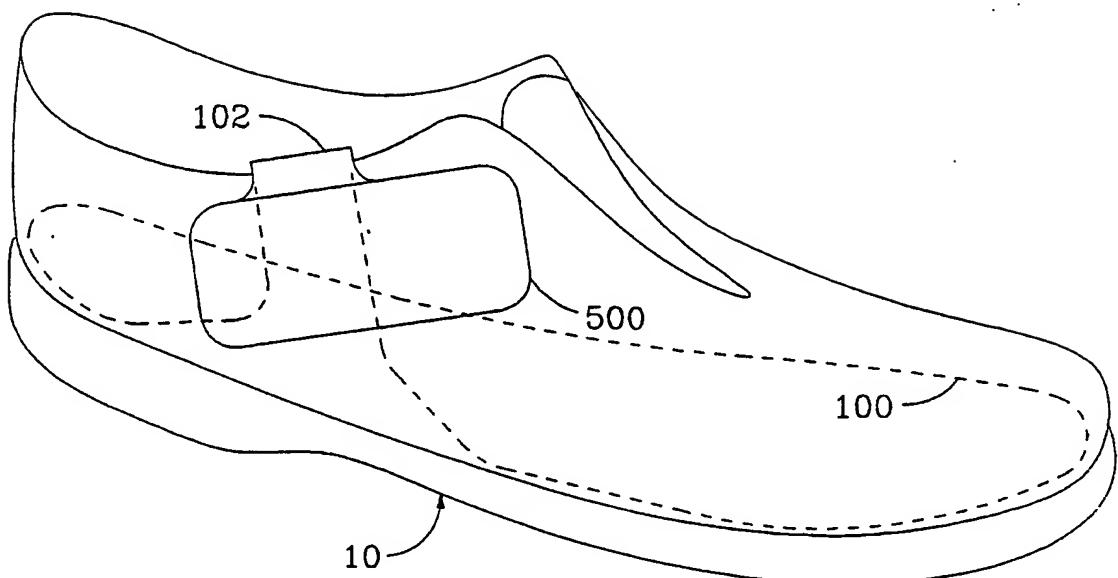


FIG. 1

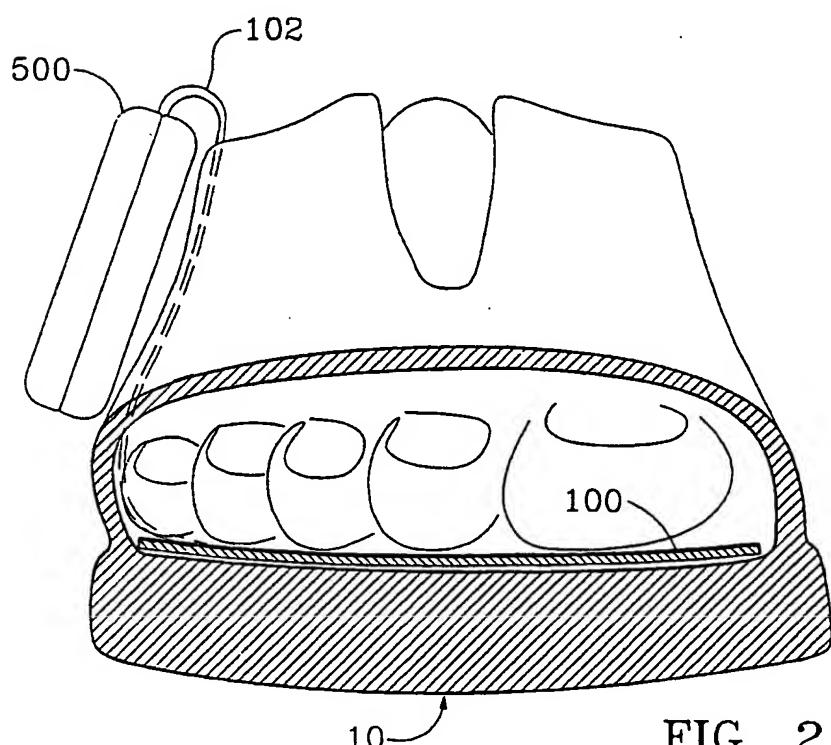
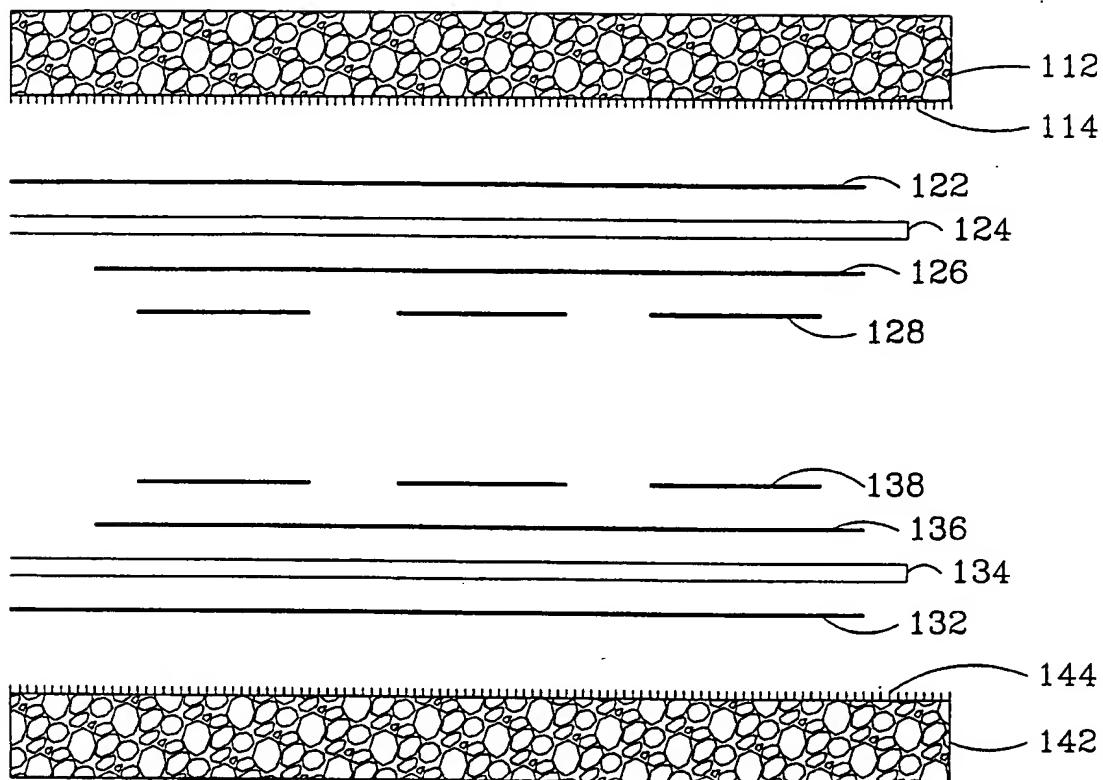


FIG. 2

2 / 10



100
FIG. 3

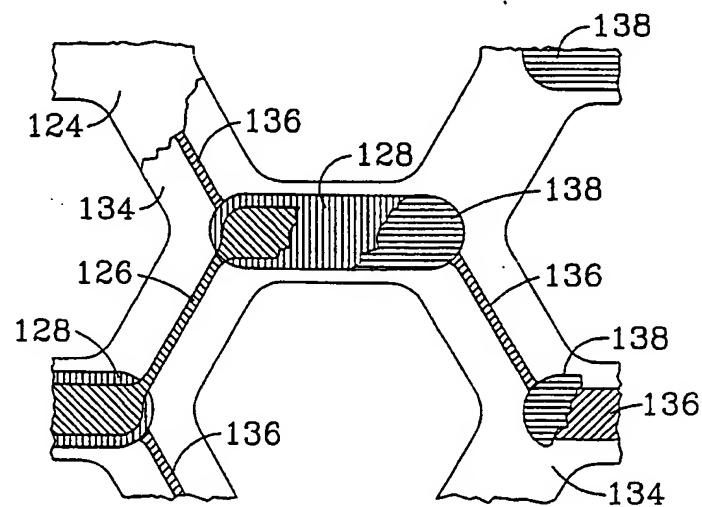


FIG. 4

3 / 10

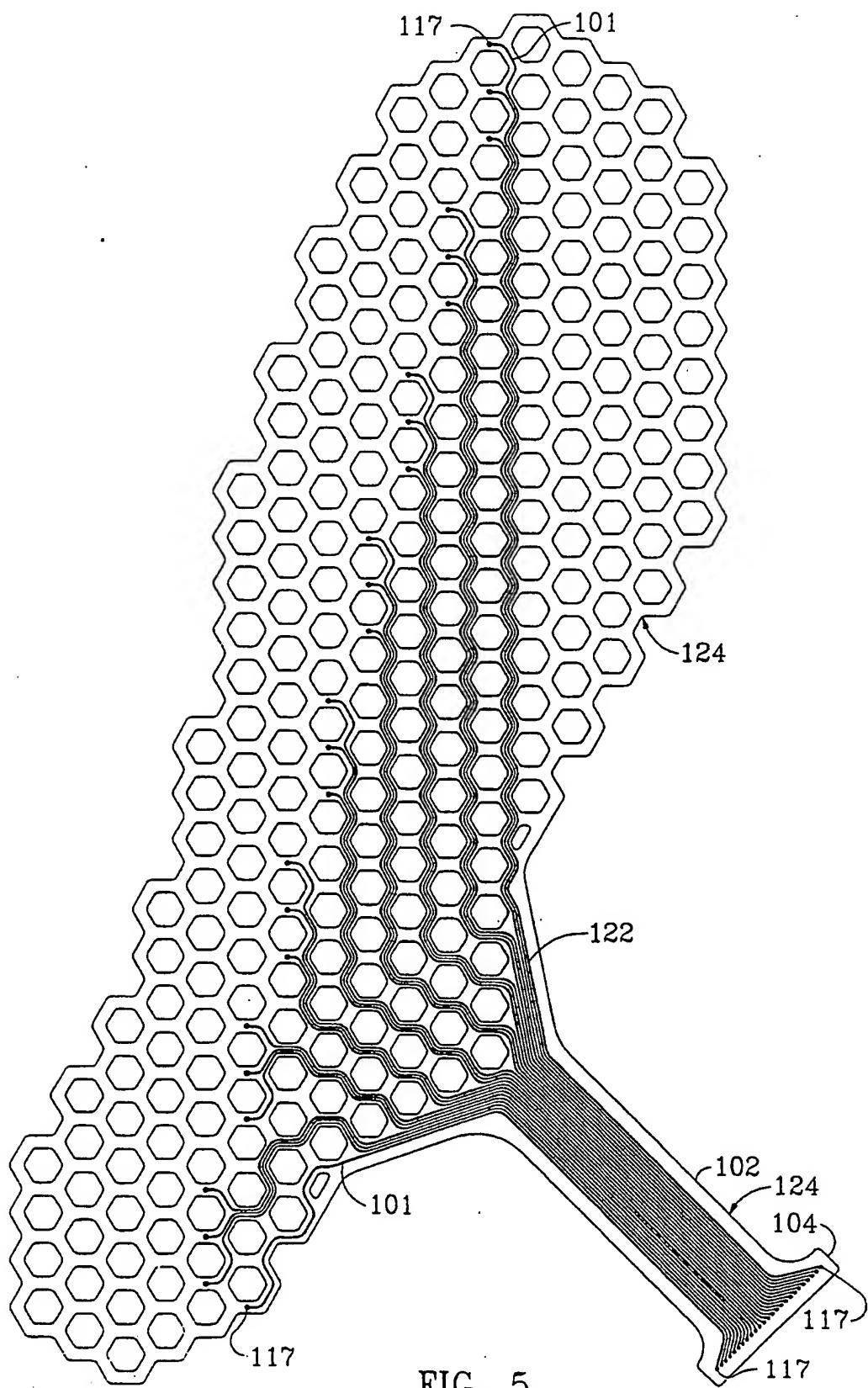


FIG. 5

4 / 10

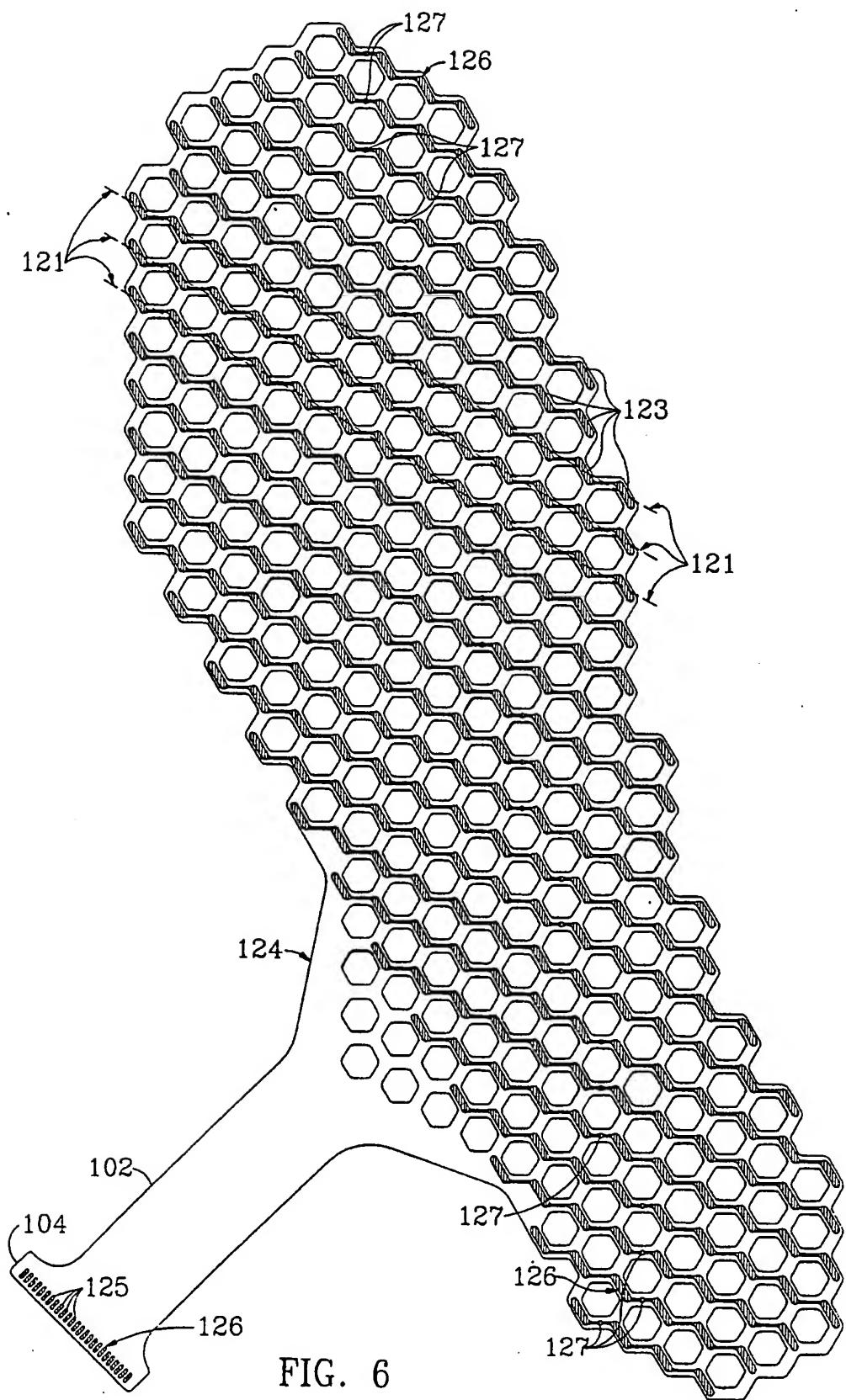


FIG. 6

SUBSTITUTE SHEET (RULE 26)

5 / 10

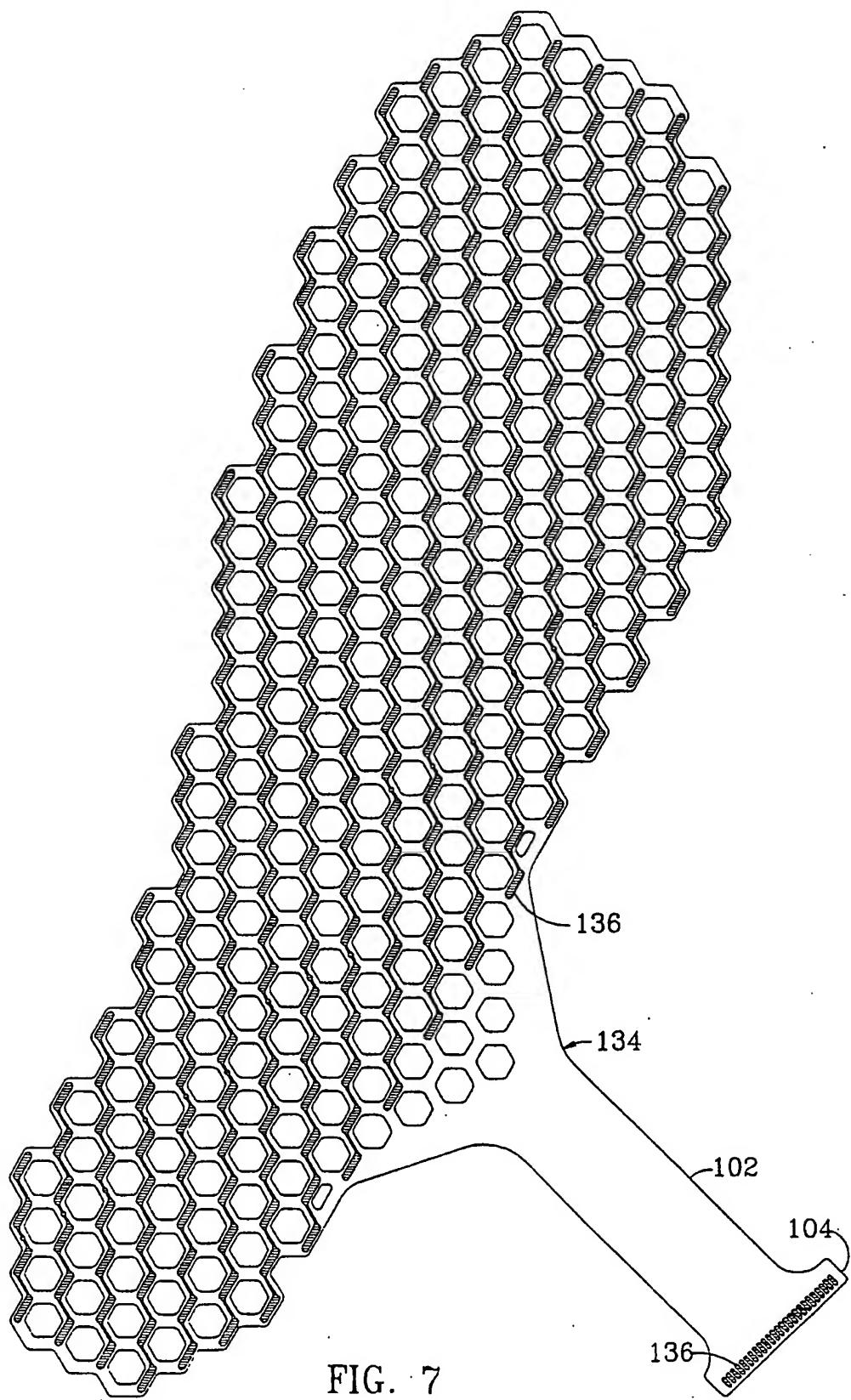


FIG. 7

SUBSTITUTE SHEET (RULE 26)

6 / 10

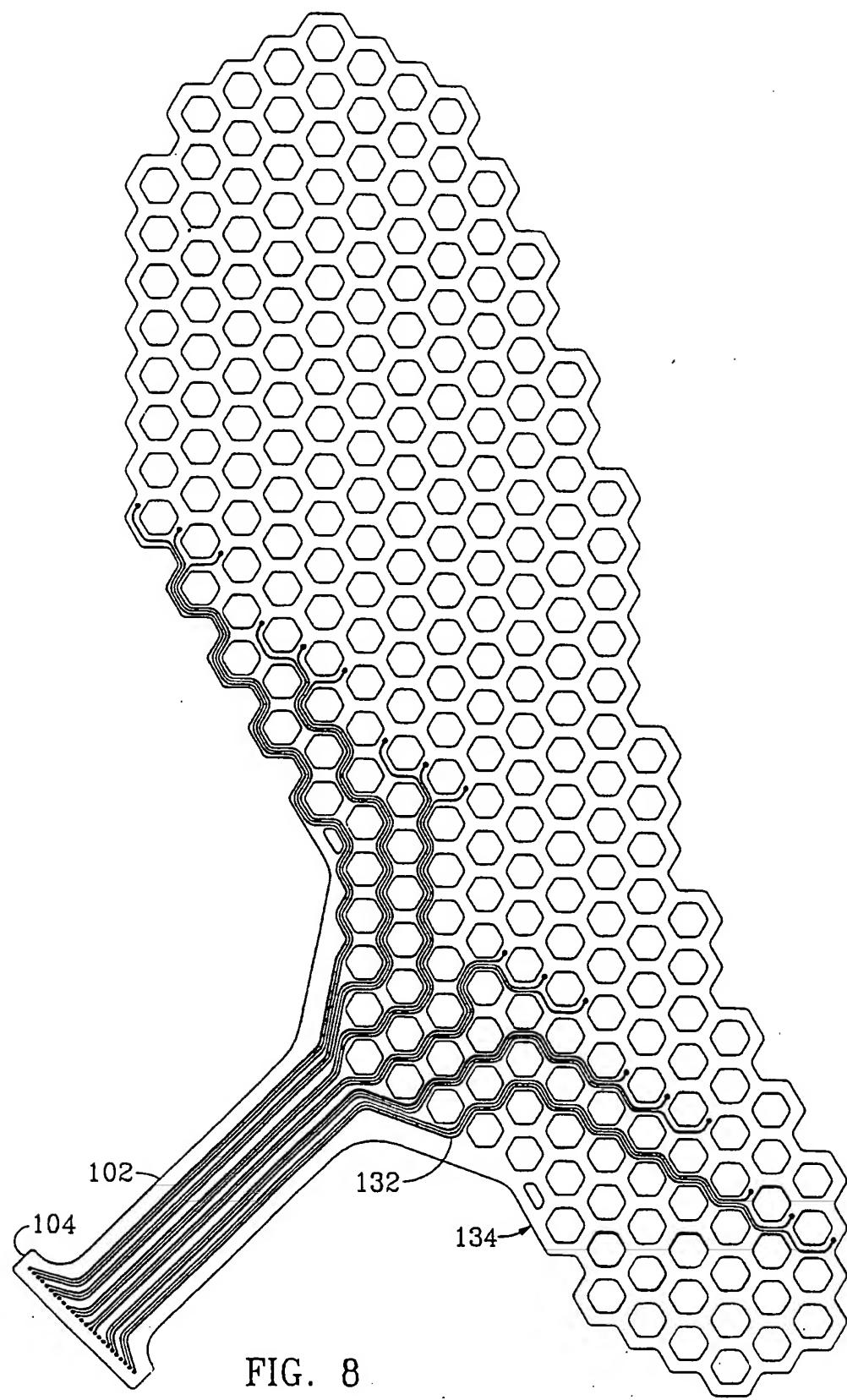


FIG. 8

SUBSTITUTE SHEET (RULE 26)

7 / 10

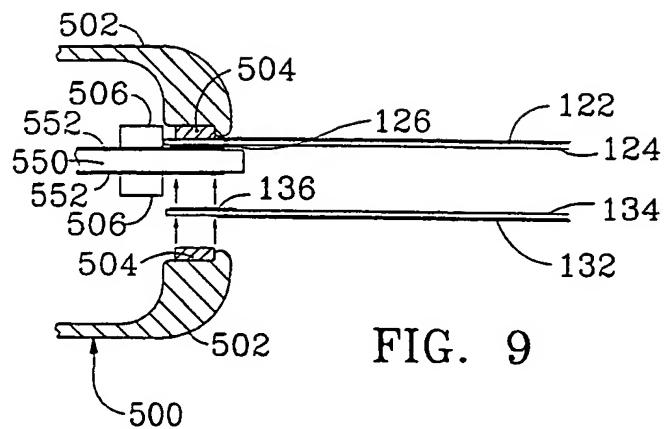


FIG. 9

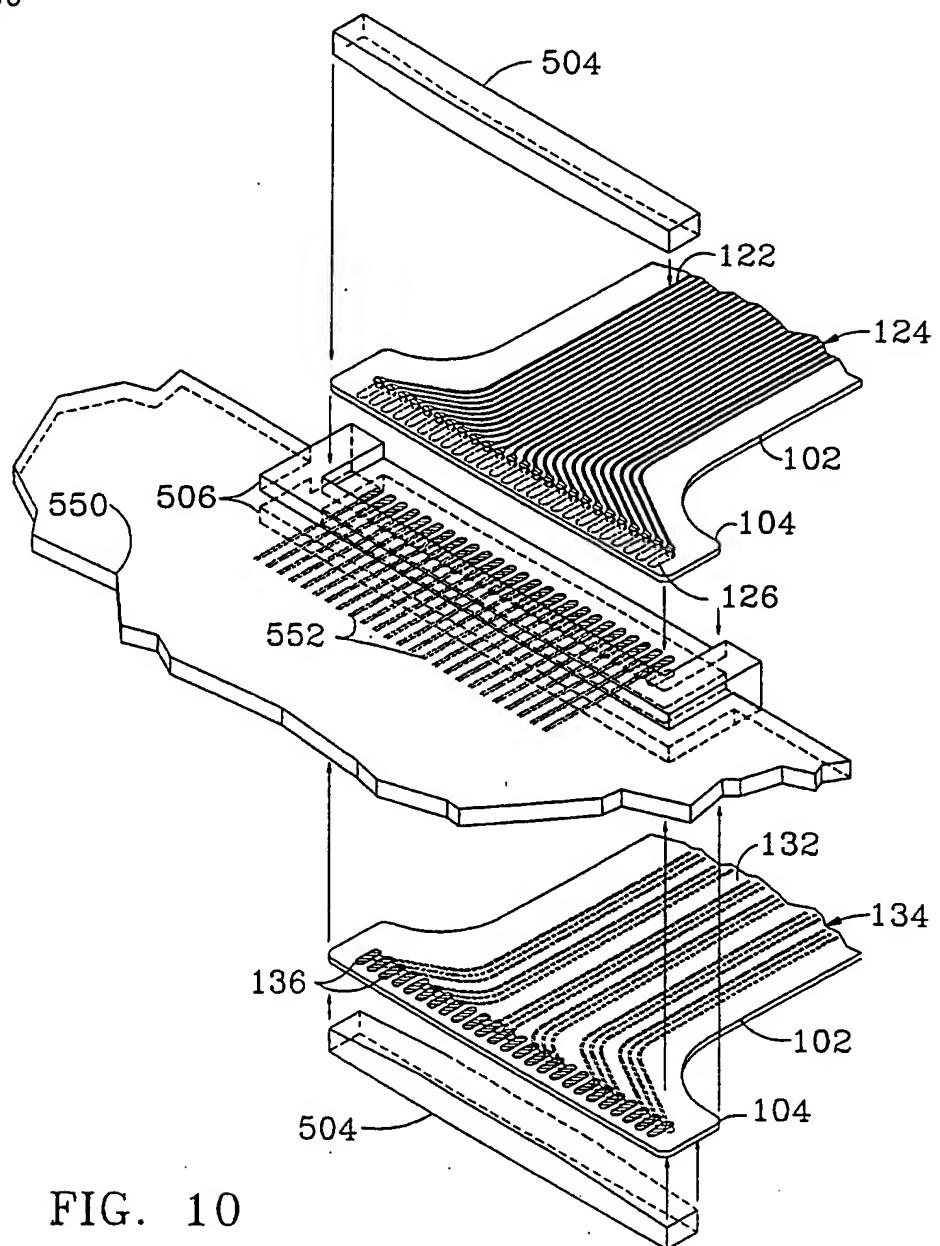


FIG. 10

SUBSTITUTE SHEET (RULE 26)

8 / 10

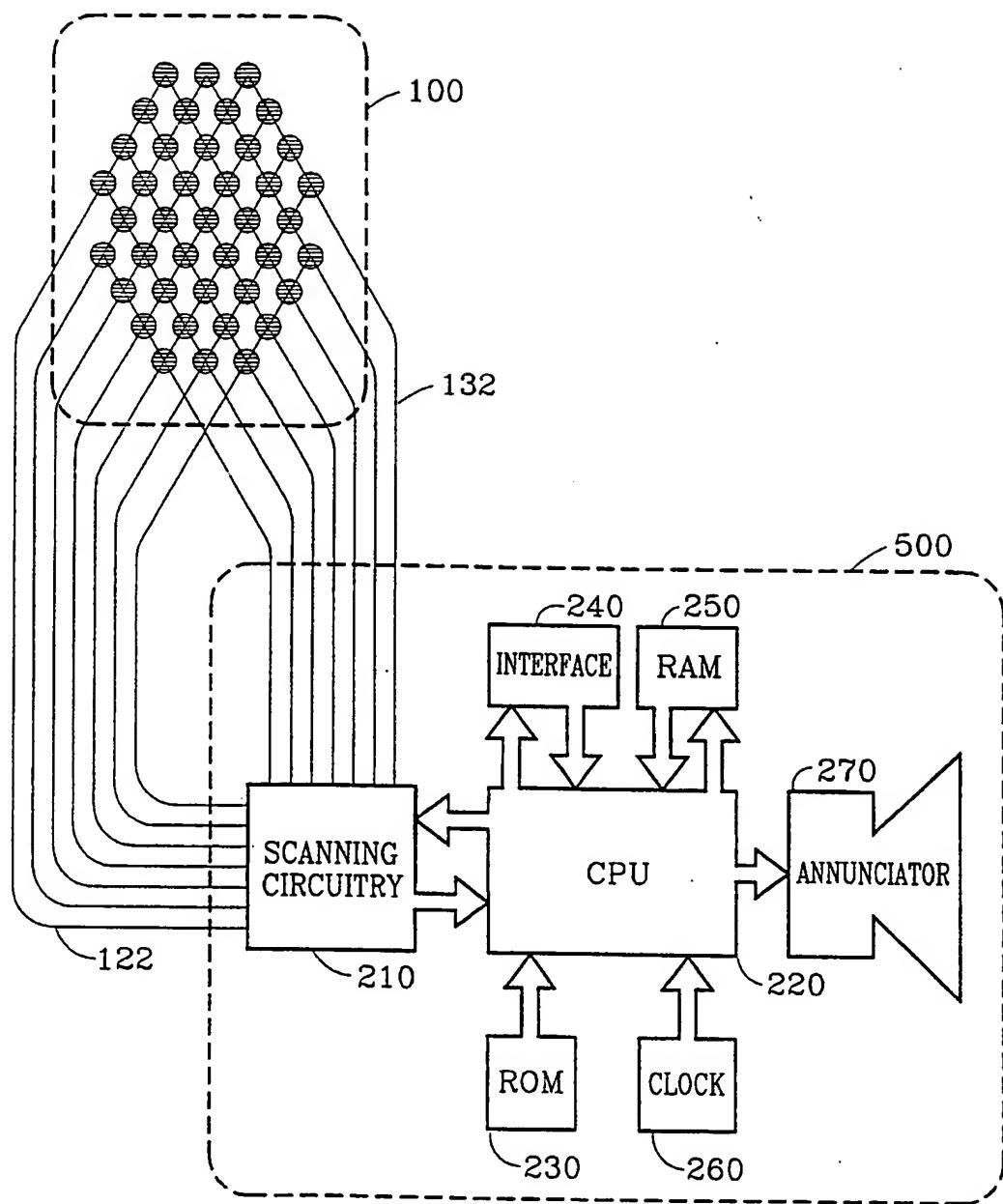


FIG. 11

9 / 10

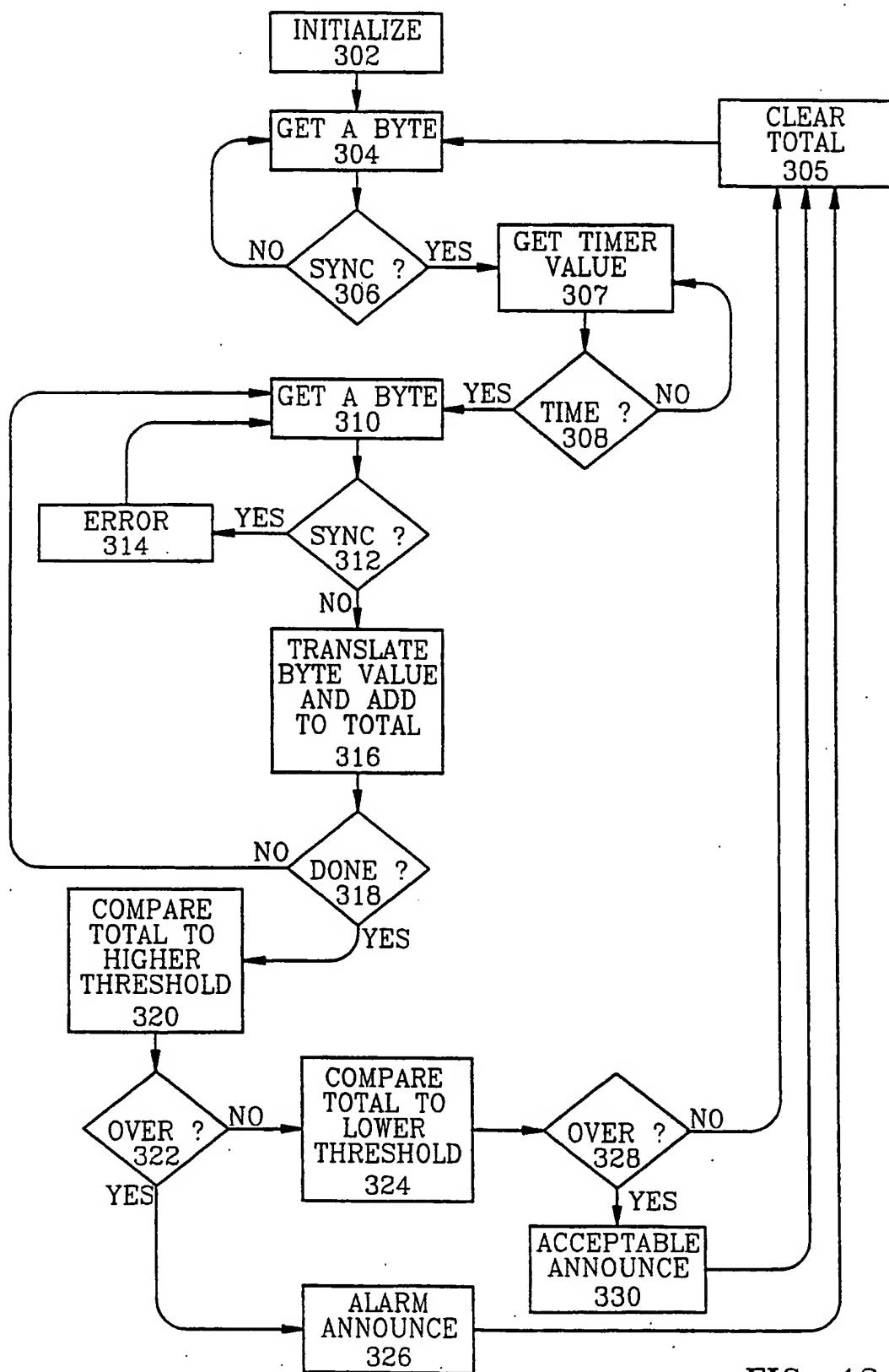


FIG. 12

SUBSTITUTE SHEET (RULE 26)

10 / 10

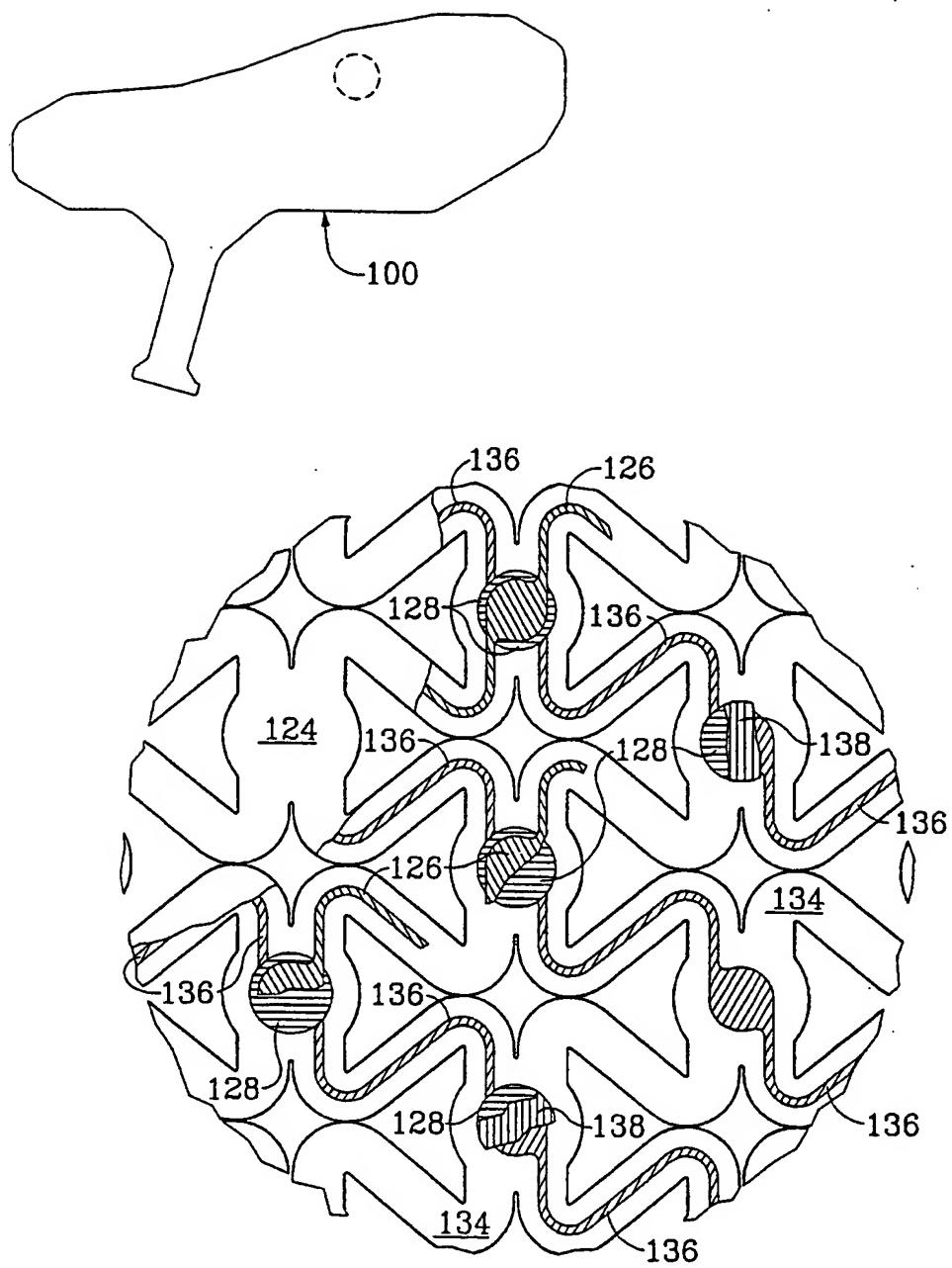


FIG. 13

SUBSTITUTE SHEET (RULE 26)

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US94/00536

A. CLASSIFICATION OF SUBJECT MATTER

IPC(5) : A61B 5/103

US CL : 073/172; 128/779

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 073/172, 862.046, 865.7; 128/779, 782; 036/132, 136, 139

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US, A 3,791,375 (Pfeiffer) 12 February 1974, See the entire document.	1-18
A	US, A, 3,974,491 (Sipe) 10 August 1976, See the entire document.	1-18
Y	US, A, 4,647,918 (Goforth) 03 March 1987, See the entire document.	1, 2, 4
A	US, A, 4,734,034 (Maness et al.) 29 March 1988, See the entire document.	1-18
X	US, A, 4,745,930 (Confer) 24 May 1988, See col. 3, lines 32-36.	1-18
A	US, A, 4,813,436 (Au) 21 March 1989, See entire document.	1-18

Further documents are listed in the continuation of Box C. See patent family annex.

Special categories of cited documents:	T	later documents published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
A document defining the general state of the art which is not considered to be of particular relevance		
E earlier document published on or after the international filing date	X	document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
L document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reasons (as specified)	Y	document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
O document referring to an oral disclosure, use, exhibition or other means	&	document member of the same patent family
P document published prior to the international filing date but later than the priority date claimed		

Date of the actual completion of the international search	Date of mailing of the international search report
07 MAY 1994	MAY 25 1994
Name and mailing address of the ISA/US Commissioner of Patents and Trademarks Box PCT Washington, D.C. 20231	Authorized officer <i>for</i> WILLIE MORRIS WORTH
Faxsimile No. (703) 305-3230	Telephone No. (703) 308-1309

Sheila H. Worthy
Patent Agent
Group 2400

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US94/00536

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US,A, 4,856,993 (Maness et al.) 15 August 1989, See col. 8, lines 12-21,	1-18
A	US, A, 4,862,743 (Seitz) 05 September 1989, See the entire document.	1-18
X	US, A, 5,033,291 (Podoloff et al.) 23 July 1991, See col. 3, line 32 through col. 6, line 32.	1-18
A	US, A, 5,079,949 (Tamori),14 January 1992, See the entire document.	1-18
X	US, A, 5,253,656 (Rincoe et al.) 19 October 1993, See col. 2, line 55 through col.3, line 54; col. 4, lines 53-66; and col. 5, lines 37-44.	1-18
X	DE, A, 26 56 864 (Lotscher et al) 11 May 1978, See figs. 1-3.	1-18
Y	DE, A 36 31 923 (Hanno) 31 March 1988, See figs 8 , 9 and 13.	1,2,4
A	Donald Endicott et al., "Leg Load Warning System for the Orthopedically Handicapped", Medical and Biological Engineering and computing(May 1974).	1-18
A	S. Miyazaki et al., "Foot-Force Measuring Device for Clinical Assessment of Pathological Gait", Medical and Biological Engineering and Computing (July 1978).	1-18
A	G. A. Spolek et al., "An Instrumented Shoe-A Portable Force Measuring Device", J. Biomechanics (Great Britain, June 1976).	1-18
A	John A. Purbrick, "A Force Transssducer Employing Conductive Silicon Rubber",First Robot Vision and Sensors Conferences, Stratford-on-Avon, England (April 1981).	1-18